# This Page Is Inserted by IFW Operations and is not a part of the Official Record

# **BEST AVAILABLE IMAGES**

Defective images within this document are accurate representations of the original documents submitted by the applicant.

Defects in the images may include (but are not limited to):

- BLACK BORDERS
- TEXT CUT OFF AT TOP, BOTTOM OR SIDES
- FADED TEXT
- ILLEGIBLE TEXT
- SKEWED/SLANTED IMAGES
- COLORED PHOTOS
- BLACK OR VERY BLACK AND WHITE DARK PHOTOS
- GRAY SCALE DOCUMENTS

# IMAGES ARE BEST AVAILABLE COPY.

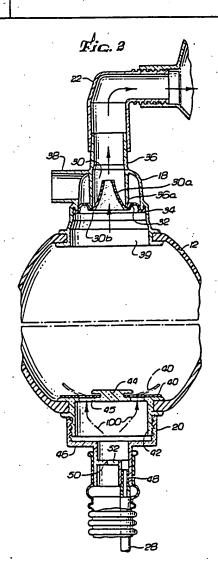
As rescanning documents will not correct images, please do not report the images to the Image Problem Mailbox.

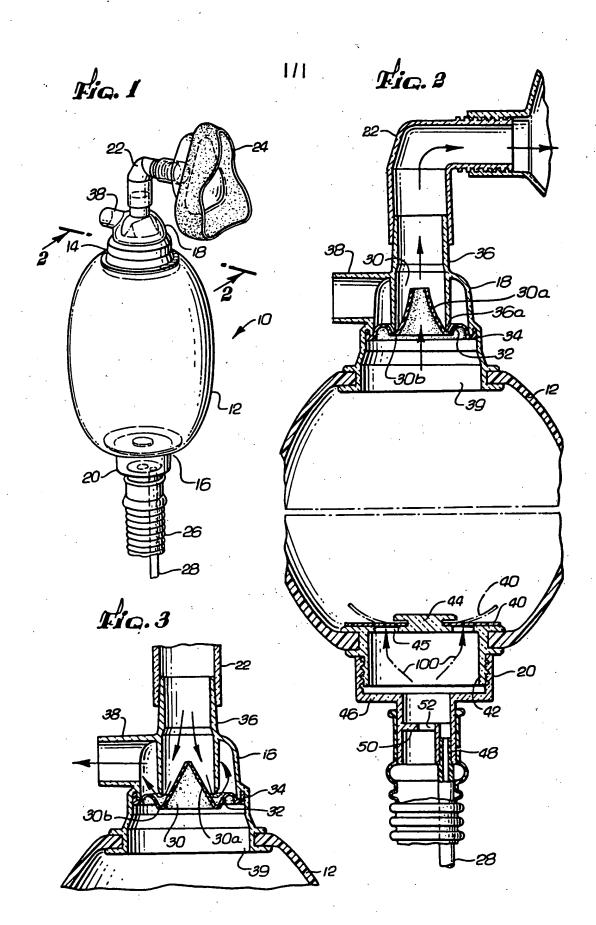
- (21) Application No 8411439
- (22) Date of filing 4 May 1984
- (30) Priority data
  - (31) 491572
- (32) 4 May 1983
- (33) US
- (71) Applicant Inspiron Corporation (USA-California), 8600 Archibald Avenue, Rancho, Cucamonga, California 91730, United States of America
- (72) Inventor Wallace Frederick Cook
- (74) Agent and/or Address for Service Haseltine Lake & Co., Hazlitt House, 28 Southampton Building, Chancery Lane, London WC2A 1AT

- (51) INT CL3 A61M 16/00
- (52) Domestic classification A5T CR
- (56) Documents cited GB 1212528
- (58) Field of search

#### (54) Resuscitator

(57) A resuscitation apparatus for use during medical procedures comprises a squeeze bag having a gas inlet and a gas outlet, and a specifically configured valve 30, 32 joined to the bag over the gas outlet. The valve housing 18 includes a squeeze bag port 39 in flow communication with the gas outlet opening, a patient port 36 and an exhalation port 38. The valve 30, 32 disposed in the housing 18 includes a portion 30a for directing fluid from the squeeze bag through the patient port 36 during inhalation or forced respiration and through the exhalation port 38 during exhalation. Another portion 30b of the valve closes off the exhalation port 38 during inhalation or forced respiration such that fluid from the squeeze bag is directed to the patient.





## **SPECIFICATION**

## Resuscitator bag

5 1. Field of the invention

This invention relates to the field of medical devices, and more particularly, to breathing equipment such as resuscitators.

10 2. Prior art

Manual resuscitators using self-inflating bags are well recognized in the prior art. Such devices are often used during "cardio-pulmonary resuscitation", often times referred to as "CPR". During such 15 procedure, it is necessary to supply the patient with large quantities of air or oxygen. In addition to forcing a volume of air to the patient, such devices must also take into account the fact that the patient may inhale or exhale under his or her own ability. As 20 a result, resuscitation bags are usually comprised of three basic components; to wit: a mask, a specific directional control valve arrangement, and a squeezable bag.

The mask is used to form a seal about the patient's 25 nose and mouth. As such, it is typically made of a soft, pliable material and is sufficiently flexible so as to contour to a wide variety of facial features. Typically, the body of the mask must be sufficiently rigid to allow uniform force to be applied so as to 30 make the seal.

The directional control valve located adjacent the mask must allow air to be forced under pressure to the patient and should also permit the patient to exhale. In addition, the valve should allow the patient to breathe spontaneously by drawing air through the bag (not forced under pressure) and to exhale.

The bag is the means for supplying air under pressure to the patient. Such bags are well known in 40 the art and generally include a one-way check valve at the end opposite the regulator valve so as to permit air to flow in one direction only into the bag. Generally, such bags should be compliant and permit 40 cycles per minute operation while deliver-45 ing a minimum of 500 cc. of air per cycle at 100 cm. of water pressure.

While each of the elements discussed above are recognized by the prior art, heretofore the prior art has created resuscitation bags and masks which had 50 various problems including complexity in design and/or operation, expense, and the like. These as well as other shortcomings have plagued this area of endeavour for a substantial period of time. Examples of prior art bags and masks are shown in U.S. Patent 55 Nos. 3,363,833; 4,037,595; 4,121,580; and 3,556,122. The present invention addresses these problems and provides a disposable bag and valve construction which are straight forward in their design, but

Summary of the invention

60

yet effective in their operation.

In the resuscitation apparatus of the present invention, a squeeze bag is provided which includes

squeeze bag port, a patient port and an exhalation port. A first valve means is disposed in the first valve housing for controlling the flow of fluid to and from the patient. The first valve means comprises a one-way valve portion for directing fluid from the squeeze bag through the patient port during inhalation or forced respiration and through the exhalation port during exhalation, and a diaphragm portion for

closing off the exhalation port during inhalation or 75 forced respiration. A second check valve means is disposed on the squeeze bag for directing fluid into the squeeze bag.

The first valve means thus enables three operations to take place: (1) "forced respiration"; (2) "free 80 exhalation"; and (3) "spontaneous breathing" through the bag. Regardless of whether there is forced respiration or spontaneous breathing by the patient, the apparatus of the present invention permits exhalation to take place.

Forced respiration is started with the pressurization of the bag. This causes the first valve means to seal the exhalation port. With the exhalation port closed off, air is forced to the patient through the patient port. The first valve means will remain in this position as long as the bag pressure is maintained greater than the atmospheric pressure. When bag pressure is removed, the first valve means will shift due to the patient lung pressure thereby opening the exhalation port for fluid flow from the patient. The 95 patient is now free to exhale through the exhalation port.

Free exhalation is achieved by directing exhaled air out of the exhalation apparatus through the exhalation port. This is also achieved by the con-100 figuration of the first valve means. This configuration is maintained as long as there is exhalation pressure.

Spontaneous breathing is permitted as the first valve means enables the patient to easily draw air 105 from the bag through the patient port. Because the first valve means in its static position seals off the exhalation port during free inhalation, the patient inhales the fluid which is in the bag. In this manner, control over the fluid directed to the patient can be 110 achieved. This valve configuration is maintained as long as the patient is inhaling. When a patient stops inhaling and starts to exhale, the first valve means shifts to permit free exhalation.

The novel features which are believed to be 115 characteristic of this invention, both as to its organization and method of operation, together with further objectives and advantages thereof will be better understood from the following description considered in connection with the accompanying drawings in which a presently preferred embodiment of the invention is illustrated by way of example. It is to be expressly understood, however, that the drawings are for the purpose of illustration and description only, and are not intended as

125 definition of the limits of the invention.

Brief description of the drawings Figure 1 is a perspective view showing the various

1日本一丁三日報は高品様子で

ď,

7

À

Figure 2 is a cut-away view of Figure 1 taken along lines 2-2 and showing the operation of the first valve means of the present invention.

Figure 3 is a cut-away view showing another 5 operation of the first valve means of the present invention.

#### Detailed description of the invention

Referring first to Figure 1, there is shown, as a 10 presently preferred embodiment of the present invention, the bag and mask assembly 10. As one can see, assembly 10 is comprised of an elongated, generally flexible squeeze bag 12 auch as is well known in the art. Typically, bag 12 is of a transparent 15 or translucent plastic and can be readily deformed with hand pressure. Bag 12 includes a first end 14 defining a gas outlet opening and a second end 16 defining a gas inlet opening. A first valve housing 18 is joined to the bag 12 adjacent the first end 14 20 thereof. Housing 18 includes a first upper bulbous section and a depending lower section joined to bag 12. A second valve housing 20 is joined to the second end 16 of the bag 12. Conduit 22 is joined to the first valve housing 18 and enables a face mask 24 25 to be joined to the bag 12 in flow communication therewith. Face mask 24 is conventional and will not be described in detail herein.

Joined to the second valve housing 20 is a flexible hose or conduit 26 which may include tubing 28.

30 Tubing 28 can be joined to an external gas source so as to regulate the type of gas being supplied to bag 12. In this manner, specific gases such as an enriched oxygen mixture and the like can be ultimately supplied to the patient as hereinbelow de-35 scribed in greater detail.

Referring now to Figures 2 and 3, one can see that valve housing 18 includes a first valve means comprising a flexible duck-billed diaphragm 30 in position by retaining snap ring 34. Duck-billed 40 diaphragm 30 is of one-piece construction comprised of a centrally located duck-billed portion 30a, an integral, generally flat concentric sealing ring portion 30b, and a flexible convolute shuttle portion 32. Duck-billed portion 30a is disposed in valve housing 45 18 such that it preferably extends up into a first patient port 36. Extending generally perpendicular

patient port 36. Extending generally perpendicular with respect to the axis of the patient port 36 is an exit port 38. Housing 18 also defines an open port 39 which surrounds the first end 14 of bag 12. Ports 36 and 39 are in flow communication with bag 12, while

50 and 39 are in flow communication with bag 12, while port 38 is in selective flow communication with the patient.

Referring now to valve housing 20, one can see that it encloses a second diaphgragm valve 40 and a 55 diaphragm body 42. Diaphragm 40 and body 42 define a one-way valve, such valves being well known in the art. In the present invention, fluid is permitted to flow into bag 12 through openings 45 only in the direction of arrows 100. Diaphragm 40 is 60 preferably mounted on protrusion 44 centrally located on body 42 as it is also conventional in the art.

A cap 46 circumferentially surrounds the body 42

and a flow control orifice 52 as hereinbelow described in greater detail.

In the operation of assembly 10, as squeeze bag 12 is depressed, internal pressure causes the di-70 aphragm 40 to press against diaphragm body 42 and thus closes off openings 100 and the second end 16 of the bag 12. Fluid within the bag 12 is therefore forced through the duck-billed valve portion 30a. port 36 and into mask 24. This is illustrated in Figure 75 2. To prevent fluid from flowing out of exit port 38, as the fluid engages the flexible diaphragm 30, it is displaced and abuts up against tubular extension or end 36a of port 36. More specifically, the generally flat concentric sealing ring 30b abuts against end 80 36a. In the preferred embodiment end 36a forms a beveled seat to insure proper sealing with ring 30b. This seals off exit port 38 with respect to the flow of fluid from the bag 12. The operation of squeezing the bag 12 to force a volume of air or other fluid to a 85 patient is generally referred to as forced respiration. If desired, conduit can be joined to a source of fluid such as oxygen or the like so as to create an oxygen rich mixture which can then be directed to the

patient.

During the free exhalation function, air or other fluid would be exhaled by the patient and flows through the conduit 22 towards the bag 12. However, such pressure causes the duck-billed valve portion 30 a to close and the sealing ring portion 30b of the flexible diaphragm 30 to move away from the end 36a of port 36. This is shown in Figure 3. In this manner, the exit port 38 is now in flow communication with port 36 and the exhalate flows through the exit port 38 to the outside. This valve configuration is maintained as long as there is an exhalation pressure.

Should the patient exhibit spontaneous breathing, the first valve means of the present invention permits this to readily take place. When the patient draws air in without the bag 12 being squeezed, the vacuum created will cause the valve diaphragm 30 to be sealed against the end 36a of port 36 and the duck-billed portion 30a to open such as is described above with respect to force respiration. The vacuum also causes the valve diaphragm 40 to open and air to flow through the bag 12 to the patient. When the patient stops inhaling and starts exhaling, the diaphragm 30 shifts to allow free exhalation as described above.

When the squeeze bag 12 is released, a vacuum is created thereby closing duck-billed portion 30a, and simultaneously opening check valve diaphragm 40.
This enables fluid to be drawn into squeeze bag 12 through openings 45. During bag refill, valve diaphragm 30 is design to permit simultaneous patient exhalation.

Yet another unique feature of this invention is the use and placement of a disk-shaped flow controller 50 defining flow control orifice 52. Controller 50 is disposed in removable cap 46. This enables one to disconnect the flow controller 50 from bag 12 should unrestricted flow into bag 12 be desired. Controller

oxygen typically cannot be supplied fast enough. Thus during bag refill, a greater-than-desired amount of air is drawn into the bag diluting the oxygen. In the present invention, oxygen is fed into 5 bag 12 through tubing 28. During bag refill, the flow of air is restricted by means of orifice 50 thus enabling more oxygen to flow into bag 12. In addition, during other operations of the bag 12, oxygen from tubing 28 flows back through orifice 52 and fills hose 26. During bag refill, hose 26 thus acts as a reservoir enabling yet additional oxygen to flow into bag 12.

Yet another feature of the present invention is that should end 16 of the bag 12 become ocluded, the 15 patient can still draw fluid through port 36. This is achieved as during inhalation with end 16 ocluded, a vacuum is formed in bag 12 thus drawing diaphragm 30 and ring 30b into bag 12. When ring 30b disengages from end 36b of port 36, fluid can then 20 be drawn into the apparatus through port 38, and directed to the patient.

While the presently preferred embodiment has been described above, it is apparent to one skilled in the art that other embodiments are also within the 25 scope of the present invention. For example, diaphragm 30 can be held in place by sealing means other than ring 34 i.e. by bonding and the like. Housing 18 can also be made in 2-parts for retaining diaphragm 30 and for easy disassembly and cleaning. Duck-billed portion 30a can also be replaced with a flapper-type check valve joined to portion 30b. In addition, other elements can be easily joined to apparatus 10 such as PEEP equipment, because of the easy access to port 38. This invention, therefore, 35 is not to be limited to the particular embodiment

### **CLAIMS**

herein disclosed.

- 40 1. A resuscitation apparatus comprising:
  - (a) squeeze bag means;
- (b) a first valve housing joined a first end of said squeeze bag means, said valve housing having a squeeze bag port, a patient port and an exhalation
   45 port;
- (c) a first valve means disposed in said first valve housing for controlling the flow of fluid to and from a patient, said first valve means comprising (i) a one-way valve portion for directing fluid from said squeeze bag, through said patient port during inhalation or forced respiration and through said exhalation port during exhalation, and (ii) a sealing portion for closing off said exhalation port during inhalation or forced respiration such that fluid from
   55 said squeeze bag is directed to the patient; and
  - (d) a second valve means disposed on said squeeze bag, said second valve means for directing fluid into said squeeze bag.
- A resuscitation apparatus according to Claim 1 60 wherein said one-way valve portion comprises a duck-billed valve disposed in said first valve housing such that at least a part of said duck bill extends into said patient port.

diaphram valve.

- 4. A resustitation apparatus according to Claim 1 further including a flexible breathing mask joined to said patient port.
- 70 5. A resuscitation apparatus according to Claim 1 further including means for directing a fluid into said squeeze bag joined to said second valve means.
- A resuscitation apparatus according to Claim 1 further including a flow controller for controlling the
   flow of fluid through said second valve means.
  - 7. In a resuscitation bag having a gas inlet opening and a gas outlet opening, the improvement comprising a valve housing joined to said bag and covering said gas outlet opening and having a
- 80 squeeze bag port in flow communication with said gas outlet opening, a patient port and an exhalation port, and a valve disposed in said housing and extending into said patient port, said valve including a check valve portion for directing fluid from said
- 85 squeeze bag through said patient port during inhalation or forced respiration and through said exhalation port during exhalation, and a portion for closing off said exhalation port during inhalation or forced respiration such that fluid from said squeeze bag is
  90 directed to the patient.
  - 8. A resuscitation bag according to Claim 7 wherein said check valve portion comprises a duck-billed valve.
- A resuscitation apparatus, substantially as
   hereinbefore described with reference to the accompanying drawing.

Printed in the UK for HMSO, D8818935, 9/84, 7102.
Published by The Patent Office, 25 Southampton Buildings, London, WC2A 1AY, from which copies may be obtained.